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# Predicting the Kinematic Response of a Helmeted Headform during Oblique Impacts

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## 6 ABSTRACT

7 160 oblique impact tests were performed to study the relationship between the kinematic response of a 8 helmeted headform and impact severity caused by the change of speed (Group 1) and anvil angle (Group 9 2). For this work, the kinematic response of a helmeted headform is evaluated by measuring linear 10 acceleration, rotational acceleration, and rotational velocity of the headform. In Group 1, a football helmet 11 was tested at 45° anvil angle at four different impact speeds ranging from 4.5m/s and 7.4m/s on five 12 impact locations. Results showed that for all cases, the relationship between impact speed and helmeted 13 headform kinematic response was linear, with an average  $R^2$  value of 0.98. At each impact location, a 14 prediction line was generated using the data points of the lowest and the highest speeds. For the speeds of 15 5.5m/s and 6.5m/s, the prediction of the helmeted headform kinematic response was validated with an 16 average error of 4.7%. In Group 2, the helmeted headform was tested at 5.5m/s impact speed at six 17 different anvil angles between 15° and 55°, and the response was fitted with a second-degree polynomial (curve) with an average  $R^2$  value of 0.96. The kinematic response of the higher and lower impact speeds 18 19 was obtained experimentally for one angle, and the fitted curve for 5.5m/s was offset to pass through the 20 obtained kinematic response. The predicted helmeted headform kinematic response was validated 21 experimentally, and the average error was found to be 8.3%. The results showed that it is possible to 22 predict the kinematic response of a helmeted headform by interpolating or extrapolating the data without 23 having to perform extra impact test. Analysis on other research works also showed similar predictable 24 behaviour for headform equipped with other helmet models. Therefore, the number of tests during the 25 process of evaluating a helmet performance can be reduced.

#### 26 KEYWORDS

Biomechanics, head injury, kinematic response, linear acceleration, rotational acceleration, footballhelmet

#### 29 INTRODUCTION

30 The protective helmet was initially developed to protect the head against severe impacts that may lead to 31 death (Hoshizaki, et al., 2014; Becker, 1998). Many studies have demonstrated that helmets are effective 32 in preventing severe head injuries such as skull fracture (McIntosh, et al., 2011; McIntosh & McCrory, 33 2005; Haider, et al., 2012; Sone, et al., 2017). However, the most common types of head injuries in sports 34 are mild traumatic brain injuries (mTBI) such as concussions (Noble & Hesdorffer, 2013). In the past, 35 head injury was thought to be caused only by the linear acceleration of the head (Hodgson & Thomas, 36 1971) However, research studies have shown that rotational acceleration plays a significant role in 37 causing head injury and concussion (King, et al., 2003; Holburn, et al., 1943; Kleiven, 2013) and majority 38 of the impacts to the head result in both linear and rotational motion of the head (Otte, 1991). Rotational 39 acceleration and velocity have a significant correlation to the brain strain response (Kleiven, 2007; 40 Rowson, et al., 2012; Ji, et al., 2014; Patton, et al., 2012), as they render shearing force to the brain 41 tissues. The brain is more susceptible to shearing forces as the bulk modulus of the brain tissues 42 (resistance to the uniform compression) is approximately one million times higher than that of the shear 43 modulus (McElhaney, et al., 1976). Furthermore, the brain deformation is more severe when the linear 44 and rotational motion were applied together (Gennarelli, et al., 1972; Ueno & Melvin, 1995; Pellman, et 45 al., 2003). Yet, helmets for decades have been tested and certified only for linear acceleration (Consumer 46 Product Safety Commission, 1998; NOCSAE, DOC, 2019; NOCSAE, DOC, 2016; UN ECE Regulation 47 22/05, 2002), and the focus has been on protecting the head against skull fractures (King, et al., 2003). 48 Since an mTBI happens more often than a skull fracture, the general populace is more concerned about 49 the concussion than the skull fracture (Vastag, 2002). As a result, standard bodies and independent 50 researchers have started to measure and analyze the rotational acceleration and rotational velocity of the 51 head, in addition to the linear acceleration, to better gauge the safety level and performance of a helmet 52 (NOCSAE, DOC, 2019; Whyte, et al., 2019). In addition, technologies were developed in recent years to 53 mitigate the injurious effects of rotational motion of the head during impacts (Aare & Halldin, 2003; 54 Halldin, et al., 2003; Abram, et al., 2019; Bliven, et al., 2019). In 2011, Virginia Tech introduced a 55 Summation of Tests for the Analysis of Risk (STAR) rating system where helmets are rated based on 56 factors such as linear acceleration, rotational acceleration, and rotational velocity response during impact 57 (Rowson, et al., 2015; Bland, et al., 2018; Rowson & Duma, 2011). Peter Halldin of MIPS also proposed 58 an oblique impact testing method in 2015 (Halldin, 2015). National Operating Committee on Standards 59 for Athletic Equipment (NOCSAE) Standard for Newly Manufactured Football Helmets introduced 60 rotational acceleration-based testing that will come into effect in November 2019 (NOCSAE, DOC, 61 2019).

- 62 Some of the helmet testing protocols require the helmet to be tested multiple times at different severity
- 63 levels gauged by the impact speed. This results in many trials, which can be expensive and time-
- 64 consuming. Finite Element Analysis (FEA) has been widely used to simulate helmet impact (Zhang, et
- al., 2004; Willinger & Baumgartner, 2003; Aare, et al., 2004; Mills, et al., 2009). FEA is a great tool for a
- 66 preliminary impact study (Fernandes & Alves de Sousa, 2013). However, in some cases, FEA results may
- 67 not be sufficiently accurate, and a physical sample of headgear is needed to experimentally validate its
- 68 performance (Fernandes & Alves de Sousa, 2013).
- 69 Several studies of helmet response showed that there are linear relationships between linear acceleration
- and impact severity. DeMarco performed impact tests of various motorcycle and cycling helmets showing
- a linear relationship between linear acceleration and impact severity as long as the helmet impact-
- absorbing liner is functional and it is not bottomed-out (DeMarco, et al., 2010; DeMarco, et al., 2016).
- 73 Cripton, Rowson, and COST 327 performed drop tests on cycling, football, and motorcycle helmets,
- respectively (Cripton, et al., 2014; Rowson, et al., 2013; Chinn, et al., 2001). However, Cripton, Rowson,
- and COST 327 did not assess the relationship between impact severity and head kinematic response.
- Furthermore, no studies have been done on the relationship between impact severity and head rotational
- acceleration and velocity (Whyte, et al., 2019). In this work, the relationship between the impact severity
- and the helmeted headform's kinematic response: linear acceleration, rotational acceleration, and
- 79 rotational velocity, is studied.

### 80 METHODS

- 81 An impact test rig was used to perform oblique impact tests at different speeds and different anvil angles.
- 82 The patent-pending impact test rig (Abram, et al., 2018) was developed and built at the Head Injury
- 83 Prevention (HIP) Lab at Simon Fraser University (SFU), Surrey, Canada. Figure 1 details the test rig. A
- 84 Hybrid III 50th percentile male dummy headform without neck was used to perform the tests.





**Figure 1.** (a) CAD model of the Oblique Impact Test Rig at the HIP Lab and (b) Oblique Impact Test Rig at the HIP Lab.

- 86 The Hybrid III headform was equipped with nine single-axis linear accelerometers (ENDEVCO 7264C,
- 87 Meggitt Sensing Systems Irvine, California) arranged on a 3-2-2-2 block array. The rotational
- 88 accelerations of the head in x, y, and z-axes during an impact were calculated with an algorithm described
- 89 in Padgaonkar (Padgaonkar, et al., 1975). Data were collected at a sampling rate of 20 kHz.
- 90 Accelerometers data were filtered through a 4th order Butterworth low-pass filter with 1000 Hz cut-off
- 91 frequency according to SAE Recommended Practice J11a (Consumer Product Safety Commission, 1998;
- 92 NOCSAE, DOC, 2017). The change in the rotational velocity was calculated through the integration of
- 93 the rotational acceleration graph.
- 94 The impact surface was a 42 Shore A Modular Elastomer Programmer (MEP) pad installed on angled
- support. The MEP pad was selected as it resembles common impact surfaces in football games (Post, et
- al., 2017; Hoshizaki, et al., 2012). The impact speed was measured using a photoelectric time gate
- 97 adjacent to the rail guide. A high-speed camera (Edgertronics SC2+) was used to record the impact tests
- 98 at 4,000 frames/sec in high definition.
- 99 A Riddell Speed football helmet (Figure 2a), Size L, was fitted according to the manufacturer's
- 100 specifications. All tests were performed without using a facemask or other accessories. The helmeted
- 101 headform was placed onto the test rig, where its orientation, position, and height were secured based on a
- 102 given impact scenario.

103 The first part of this study (Group 1) focused on changing the speed of impact while keeping the angle of

104 impact fixed at 45°. Five impact locations were selected for Group 1 based studies on the most prevalent

105 impact locations (Pellman, et al., 2003; Crisco, et al., 2010; Daniel, et al., 2012): Front-Top (FT), Front-

106 Boss (FB), Front-Y (FY), Lateral-X (LX), and Side-Back (SB). The impact locations can be seen in

- 107 Figure 2b-d. At each impact location, data points was obtained at speeds of 4.5, 5.5, 6.5, and 7.4 m/s. To
- 108 obtain a data point, five tests with results within 10% of each other are required. In total, 100 tests were
- 109 conducted for Group 1 testing.



**Figure 2.** (a) The Riddell Speed football helmet, (b) front-top FT impact location, front FY impact location, front-boss FB impact location, (c) side-back SB impact location, and (d) lateral LX impact location.

110 The results of Group 1 testing, including linear acceleration, rotational acceleration, and rotational

111 velocity at different speeds, were examined while keeping the impact angle fixed. A regression analysis

112 was performed on the result of Group 1. The data were fitted with a first-order polynomial (Equation 1).

113

$$y = a_1 x + a_0 \quad , \quad a_n \neq 0 \tag{1}$$

Then, for each kinematic response at every impact location (one set of data), in Group 1, any combination of two out of four data points was selected, and Equation 1 was fitted through the two selected data points to obtain the prediction line.

117 The experimental and predicted values of the kinematic response for the other two points were compared.

118 The percent (%) error represents the difference between experimental and predicted values and was

119 calculated with Equation 2.

120 % 
$$Error = \left|\frac{Experiment - Prediction}{Experiment}\right| \times 100\%$$
 (2)

121 Also, COST 327 reported oblique impact testing of four different models of motorcycle helmets for five

122 different speeds from 6m/s to 12m/s without analyzing the relationship between impact speed and

kinematic response (Chinn, et al., 2001). As a part of this study, the results of COST 327 were alsoanalyzed.

125 In the second part of this study (Group 2), the angle of impact varied while the speed of the impact was

126 fixed, at speed recommended by NOCSAE, 5.5m/s (NOCSAE, DOC, 2019). One impact location, FY,

127 was chosen for all tests. One set of impact test was conducted on six anvil angles between 15°, 22°, 30°,

128 37°, 45°, and 55°, yielding six data points for each set. In addition, two sets of impact tests, one tested at

129 4.5m/s and the other 6.5m/s were also conducted on three anvil angles (15°, 30°, and 45°), yielding three

130 data points per set. With five trials for each impact scenario, 60 tests were conducted in total.

131 Similar to Group 1 test, the results of Group 2 testing, including linear acceleration, rotational

132 acceleration, and rotational velocity at different angles, were examined while keeping the impact speed

133 fixed. To obtain a data point, five tests with results within 10% of each other are required. In total, 60

tests were conducted for Group 2 testing. A regression analysis was performed on the result of Group 2

135 from fixing the speed at 5.5 m/s. The 5.5 m/s data were fitted with a second-order polynomial (Equation

136 3).

137

$$y = a_2 x^2 + a_1 x + a_0 , \ a_n \neq 0$$
(3)

138 The generated curve from 5.5m/s impact speed was used to predict the kinematic response for 4.5m/s and 6.5m/s impact speeds. At each speed level, the curve was offset to pass through one experimental data 139 140 point. The prediction line was used in three different scenarios. In scenario 1, the prediction line passed 141 through the experimental data points of 15°. In scenario 2, the prediction line passed through the 142 experimental data points of 30°, in scenario 3, the prediction line passed through the experimental data 143 points of 45°. For example in scenario 2, as shown in Figure 5a-c, the curve obtained from 5.5m/s speed 144 was offset to pass through only the 30° data points to predict the kinematic response for impact speeds of 145 4.5 m/s and 6.5 m/s for the  $15^{\circ}$  and  $45^{\circ}$ . Then, the prediction was validated by comparing the predicted and 146 experimental values. The percent (%) error was calculated with Equation 2.

147 RESULTS

148 Group 1 comprises of testing on five locations of the football helmet for four different speeds between

149 4.5m/s and 7.4m/s. The results of the impact tests at different impact locations were summarized in Table

- 150 1. The Coefficient of Variation (CV) was computed from the standard deviations and mean values of each
- 151 measured kinematic parameter.
- 152

Impact speed (m/s)	Lin.Acc. (g)	Lin. Acc CV (%)	Rot. Acc. (krad/s²)	Rot. Acc. CV (%)	Rot. Vel. (rad/s)	Rot. Vel. CV (%)							
	FY												
4.5	81.52	3.13	3.53	9.37	24.25	1.86							
5.5	94.60	2.74	5.02	2.59	29.57	7.05							
6.5	124.73	3.76	6.28	8.24	36.06	4.20							
7.4	142.00	0.98	7.78	7.17	39.90	3.36							
			LX										
4.5	68.64	2.57	3.32	8.21	23.71	3.25							
5.5	73.84	3.69	4.18	4.91	29.79	6.72							
6.5	103.84	3.22	5.30	5.17	36.74	3.34							
7.4	125.72	1.41	6.67	9.78	36.18	2.49							
	1	1	FT										
4.5	64.58	2.19	3.01	2.26	24.00	1.43							
5.5	81.76	2.38	3.82	3.87	29.22	1.01							
6.5	100.60	1.32	4.68	8.41	34.08	2.57							
7.4	120.57	3.83	5.97	4.53	40.48	1.52							
			FB										
4.5	86.85	2.21	3.75	8.64	26.83	5.67							
5.5	107.39	2.83	4.46	3.88	31.64	2.79							
6.5	125.30	3.05	5.53	1.88	37.10	3.44							
7.4	139.18	2.47	6.58	2.80	40.62	2.32							
			SB										
4.5	53.05	2.22	3.47	4.54	24.56	3.18							
5.5	67.87	2.19	3.79	3.12	25.63	3.82							
6.5	81.94	3.83	5.70	3.60	39.99	4.09							
7.4	98.90	4.69	6.17	1.99	43.94	2.61							

153 **Table 1.** Average responses of the headform when impacting different areas of the helmet at various speeds.

- 155 Figure 3a-c show the Group 1 data points fitted with Equation 1. The R<sup>2</sup> values for the best-fitted line for
- all five impact locations were calculated. The average  $R^2$  values for linear acceleration, rotational
- acceleration, and rotational velocity were 0.9855, 0.9809, and 0.9595, respectively. The equation
- 158 parameter and the R<sup>2</sup> values were summarized in Table 2. The equation parameter p-value was also
- 159 calculated. A p-value less than 0.05 is statistically significant.

			Lin. Acc.		
Loc.	<i>a</i> <sub>1</sub>	p-value	<i>a</i> <sub>0</sub>	p-value	<b>R</b> <sup>2</sup>
FY	21.6104	0.0033	-18.4855	0.1414	0.9867
LX	20.6462	0.0203	-29.6601	0.2432	0.9545
FT	19.2042	0.0029	-22.8203	0.0796	0.9993
FB	18.5087	0.0056	3.7941	0.3664	0.9973
SB	15.3209	0.0051	-15.6712	0.1415	0.9899
		Rot	. Acc.		
Loc.	<i>a</i> <sub>1</sub>	p-value	<i>a</i> <sub>0</sub>	p-value	<b>R</b> <sup>2</sup>
FY	1.4200	0.0055	-2.8365	0.0492	0.9879
LX	1.1397	0.0077	-1.9073	0.0908	0.9924
FT	1.0020	0.0117	-1.6165	0.1503	0.9883
FB	1.0042	0.0036	-0.9365	0.1928	0.9855
SB	1.0359	0.0250	-1.3744	0.3068	0.9505
		Rot	t. Vel.		
Loc.	<i>a</i> <sub>1</sub>	p-value	<i>a</i> <sub>0</sub>	p-value	<b>R</b> <sup>2</sup>
FY	5.4588	0.0019	-0.1927	0.9443	0.9997
LX	4.5123	0.0563	4.7947	0.5735	0.8683
FT	5.5777	0.0068	-1.3656	0.8329	0.9956
FB	4.9605	0.0020	4.3257	0.0472	0.9993
SB	7.5144	0.0332	-11.1584	0.3193	0.9347

160 **Table 2.** Equation parameters and the coefficients for the best fit lines of the response for Group 1.

161

- 162 Figure 3d-f showed the prediction line obtained from fitting the data points of the lowest and higest speed
- 163 with Equation 1. Table 3 compares the experimental and predicted values of the helmeted headform
- 164 kinematic response for the other two points.

6I	Lin. Acc. (g)		Rot.	Acc. (kra	d/s²)	Rot. Vel. (rad/s)			
Speed (m/s)	Experi ment	Predict ion	% Error	Experi ment	Predict ion	% Error	Experi ment	Predict ion	% Error
				F	Y		_		
5.5	94.60	101.47	7.3	5.02	4.93	1.8	29.57	29.41	0.5
6.5	124.73	126.22	1.2	6.28	6.67	6.2	36.05	35.81	0.7
				L	X				
5.5	73.84	86.23	16.8	4.18	4.35	4.1	29.79	27.56	7.5
6.5	103.84	106.68	2.7	5.30	5.55	4.7	36.74	32.02	12.8
				F	Т			•	
5.5	81.76	81.68	0.1	3.82	3.91	2.4	29.22	29.04	0.6
6.5	100.60	101.88	1.3	4.68	4.98	6.4	34.08	34.98	2.6
	•			. F	B			1	
5.5	107.39	104.85	2.4	4.46	4.72	5.8	31.64	31.57	0.2
6.5	125.30	124.46	0.7	5.53	5.78	4.5	37.10	36.74	1.0
	•			S	В		•		
5.5	67.87	66.47	2.1	3.79	4.26	12.4	25.63	30.23	17.9
6.5	81.94	85.49	4.3	5.70	5.38	5.6	39.99	38.27	4.3

167	Table 3.	Comparison	of the experimental	versus predicted v	alues of Group 1.
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**Figure 3.** Plots of speeds versus (a) linear acceleration, (b) rotational acceleration, and (c) rotational velocity fitted with a polynomial degree 1 through all points and plots of speeds versus (d) linear acceleration, (e) rotational acceleration, and (f) rotational velocity fitted with a polynomial degree 1 through points from speeds of 4.5m/s and 7.4m/s.

- 169 The results of COST 327 were plotted, as shown in Figure 4a-b. The R<sup>2</sup> values for the rotational
- acceleration of the four helmet models were between 0.9903 and 0.9991. For rotational velocity, the R<sup>2</sup>
- 171 values were between 0.8995 and 0.9952.



**Figure 4.** Plots of speeds versus (a) rotational acceleration, (b) rotational velocity of four motorcycle helmets from COST 327 report (Chinn, et al., 2001).

- 173 Group 2 comprises of testing on six different anvil angles between 15° and 55° at a fixed impact speed of
- 174 5.5m/s and one impact location, FY. The results of the impact tests were summarized in Table 4.
- 175 **Table 4.** Average responses of the helmeted headform struck at the FY region at 5.5m/s, 4.5m/s, and 6.5
- 176 m/s with varying angles.

Impact angle (°)	Linear Acc (g)	Lin. Acc. CV	Rot. Acc (krad/s²)	Rot. Acc. CV	Rotational velocity (rad/s)	Rot. Vel. CV
			5.5m/s			
15	44.74	2.78	4.69	4.39	34.23	2.20
22	65.24	2.69	5.16	4.37	35.99	3.06
30	82.10	1.90	5.36	1.36	34.24	0.92
37	90.85	1.78	5.13	6.14	31.72	4.17
45	95.98	5.41	4.94	2.41	28.94	3.68
55	110.45	2.73	3.88	6.94	27.56	5.73
			4.5m/s	<b>b</b>		
15	32.97	2.90	3.42	5.47	27.50	1.88
30	62.19	4.33	4.51	4.01	27.49	4.19
45	81.52	3.13	3.53	9.37	24.25	1.86
			6.5m/s			
15	53.93	9.73	5.46	7.97	41.28	1.14
30	94.26	4.88	6.39	3.71	39.72	3.62
45	124.73	3.76	6.28	8.24	36.05	4.20

177

178	Group 2 results	were plotted in	Figure 5a-c,	including the	fitted polynomial	and the prediction	line (of
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179 scenario 2). The equation parameter and the  $R^2$  values were also summarized in Figure 5a-c. The

180 experimental and the predicted values for all scenarios were compared shown in Table 5.



**Figure 5.** Plotting scenario 2 prediction results: (a) linear acceleration, (b) rotational acceleration, and (c) rotational velocity.

182	Table 5.	Comparison	of the	experimental	versus predicted	values of	Group 2.
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	Angle	I		g)	Rot.	Acc. (kra	d/s²)	Ro	t. Vel. (rad	l/s)
	(°)	Experi ment	Predict ion	% Error	Experi ment	Predict ion	% Error	Experi ment	Predict ion	% Error
					4.5	m/s				
	30.0	62.19	66.16	6.4	4.51	4.04	10.5	27.49	25.82	6.1
urio 1	45.0	81.52	87.31	7.1	3.53	3.55	0.8	24.25	22.40	7.6
Scens					6.5	m/s				
•1	30.0	94.26	87.12	7.6	6.39	6.08	4.8	39.72	39.61	0.3
	45.0	124.73	108.27	13.2	6.28	5.60	10.9	36.05	36.18	0.4
					4.5	m/s				
	15.0	32.97	29.01	12.0	3.42	3.89	13.8	27.50	29.17	6.1
ırio 2	45.0	81.52	83.34	2.2	3.53	5.03	14.2	24.25	24.07	0.7
Scens					6.5	m/s				
	15.0	53.93	61.07	13.2	5,46	5.77	5.7	41.28	41.39	0.3
	45.0	124.73	115.40	7.5	6.28	5.91	5.9	36.05	36.30	0.7
nar 3					4.5	m/s				
Sce	15.0	32.97	27.19	17.5	3.42	3.39	0.9	27.50	29.35	6.7

30.0	62.19	60.38	2.9	4.51	4.01	11.1	27.49	27.67	0.7
				6.5	m/s				
15.0	53.93	70.39	30.5	5.46	6.14	12.5	41.28	41.15	0.3
30.0	94.26	103.58	9.9	6.39	6.77	5.9	39.72	39.48	0.6

## 184 DISCUSSION

185 When the speed of impact is increased, linear acceleration, rotational acceleration, and rotational velocity

186 of the helmeted headform increase proportionally. As shown in the results of Group 1 in Table 1, while

187 keeping the anvil angle fixed at 45°, increasing the speed of impact from 4.5m/s to 7.4m/s increased the

linear acceleration from 81.52 g to 142.00 g for the FY location, 68.64 g to 125.72 g for the LX location,

189 64.58 g to 120.57 g for the FT location, 86.85 g to 139.18 g for the FB location, and 53.05 g to 98.90 g

190 for the SB location. A similar increasing trend can be observed for rotational acceleration and rotational

191 velocity. When the speed of impact was increased from 4.5m/s to 7.4m/s, the rotational acceleration of

192 FY, LX, FT, FB and SB test increased respectively from 3.53 krad/s<sup>2</sup> to 7.78 krad/s<sup>2</sup>, 3.32 krad/s<sup>2</sup> to 6.67

193 krad/s<sup>2</sup>, 3.01 krad/s<sup>2</sup> to 5.97 krad/s<sup>2</sup>, 3.75 krad/s<sup>2</sup> to 6.58 krad/s<sup>2</sup>, 3.47 krad/s<sup>2</sup> to 6.17 krad/s<sup>2</sup>. The linearity

194 observed was in concert with the results presented by Cripton, Rowson, and DeMarco.

195 As shown in Figure 3d-f, the result showed that the overall best result for predicting the other two speeds'

196 kinematic response was achieved when the data points from the lowest (4.5m/s) and the highest speeds

197 (7.4m/s) were chosen. The average error generated from predicting the helmet response at 5.5m/s and

198 6.5m/s in all impact locations was 4.7%, with a minimum error of 0.1% and a maximum error of 17.9%.

199 The results of COST 327 also showed that, when the speed of impact varies, the kinematic response of a

200 helmeted headform behaves linearly. The linear behaviour was observed for the peak rotational

201 acceleration and the peak rotational velocity versus the speed of impact. However, COST 327 did not

202 report peak linear acceleration in their study.

In Group 2, as shown in Table 4, fixing the speed at 5.5m/s while increasing the angle from 15° to 55°

resulted in an overall increase of linear acceleration from 44.74 g to 110.45 g. On the other hand, a mixed

205 trend in rotational kinematics was observed. Rotational acceleration, unlike linear acceleration and

206 rotational velocity, did not always increase. There was a maximum (most severe) rotational acceleration

within the specidied angles of impact (between 15° to 55°), which happened at around 30°. The rotational

acceleration increased from 4.69 krad/s<sup>2</sup> (at  $15^{\circ}$ ) to 5.46 krad/s<sup>2</sup> (at  $30^{\circ}$ ), then decreased to 3.88 krad/s<sup>2</sup> (at

209 55°). The rotational velocity increased from 34.23 rad/s (at 15°) to 35.99 rad/s (at 22°) and then decreased

210 gradually to 27.56 rad/s (at 55°). The results of Group 2 testing showed a relationship between the

- 211 kinematic response and the anvil angle when the speed of impact was fixed at 5.5m/s. The relationship
- 212 was best described by a second degree-polynomial (Equation 3).
- 213 According to the results shown in Figure 5a-c, a second degree-polynomial was adequate with R<sup>2</sup> values
- of 0.99, 0.98, and 0.90 for linear acceleration, rotational acceleration, and rotational velocity, respectively.
- The equation parameters,  $a_2$ ,  $a_1$ , and  $a_0$ , for linear acceleration are -0.0268, 3.4169, and 1.2784,
- respectively. For rotational acceleration, the equation parameters are -0.0025, 0.1523, and 2.9726,
- respectively. The equation parameters for rotational velocity are -0.0039, 0.0625, 35.1562, respectively.
- 218 The results in Table 5 showed that in scenario 1, the response was predicted with an average error of
- 219 6.3%. In scenario 2, the average error of the prediction response was 6.9%. In scenario 3, the average
- prediction error was 8.3%.

In total, 160 impact tests were performed with one type of football helmet. It was also observed that the

222 kinematic response of the headform equipped with that specific helmet can be predicted. The prediction

model can be used to reduce the number of data points that need to be obtained experimentally. Since the

results presented from the other studies on different helmets showed linear behaviour, one can conclude

that kinematic response of the helmeted headform can be predicted in most cases as long as the shock-

absorbing liner of the helmet is functional and is not bottomed out.

227 In this study, impact tests were performed using the oblique impact drop test rig with a neckless Hybrid 228 III headform. The NOCSAE standard for newly manufactured football helmet recommend both the linear 229 impactor test and the drop test. However, unlike drop test, linear impactor tests produce little tangential 230 force (Willinger, et al., 2015), a crucial contributor to the rotational acceleration of the head (Finan, et al., 231 2008). NOCSAE linear impactor test also calls for the use of a Hybrid III neck. Studies on the Hybrid III 232 neck showed that Hybrid III neck is too stiff (Herbst, et al., 1998) compared to the human neck. In 233 addition, the Hybrid III neck is designed only for flexion and extension (Svensson & Lovsund, 1992) and 234 its behaviour for other types of motion such as lateral is not known (Aare & Halldin, 2003; Bartsch, et al., 235 2012; Myers, et al., 1989; Gwin, et al., 2009). A study on helmeted head impact suggested that for the 236 first 10 ms of an impact, the effect of the neck is minor (Willinger, et al., 2015). Another study showed 237 that it takes 13–14 ms for the muscles of the human neck to respond to an impact to the head (Kuramochi, 238 et al., 2004). A typical acceleration pulse in football helmet impact lasts for approximately 15 ms and may 239 not result in a resisting response from the neck muscles (Pellman, et al., 2003; Zhang, et al., 2004; Deck 240 & Willinger, 2008). Also, there is an atlanto-occipital zone where the neck joint can have motion in the 241 range of 10° without affecting the kinematic response of the head (Ivancic, 2014; Camacho, et al., 1997). 242 Therefore, using a drop test and a neckless headform seems to be more realistic than using a linear 243 impactor test with a Hybrid III head and neck for performing oblique impact tests.

244 This study also comes with some limitations, with the main limitation being only one helmet type was

- used: football helmet. In Group 1, results from other research studies on motorcycle and bicycle helmets
- were analyzed and similar linearity was observed. However, in Group 2, testing at more angles, locations,
- and speeds with different helmet models is required. Tests with different apparatus, such as NOCSAE
- headform which is more anthropomorphically correct than a Hybrid III, may also be done in the future.

#### 249 CONCLUSION

250 The relationship between impact speed, impact angle and the kinematic response of a helmeted headform 251 was studied. It was observed that when the speed of impact was varied, and the angle of impact was fixed, 252 the kinematic response behaved linearly. This linear behaviour was then used to predict the response for 253 different speeds with an average error of 4.7%. On the other hand, when the angle of impact was varied, 254 and the impact speed was fixed, the kinematic response of the helmeted headform was best described with 255 a second-degree polynomial (curve). Then, the kinematic response was predicted and validated at 256 different speeds. The result showed that the average error of the prediction was from 6.3% to 8.3%. The 257 prediction model can be used to reduce the number of data points that need to be obtained experimentally. 258 When examining and rating a helmet performance, one can test the helmet at different speeds or angles 259 and use this prediction method to obtain more data points at other speeds and angles. Although, it is 260 known that by increasing the speed, the linear and rotational acceleration increase as well, but the rate of 261 change is not one-to-one. In this study, three different helmet types (football, motorcycle, and bicycle) 262 were examined, and the results can help other researchers to have an educated guess regarding the 263 performance of a helmet in different impact speeds. Particularly, this study shows that the rotational 264 acceleration of a football helmet does not have a linear behaviour when the angle of impact increases. A 265 peak rotational acceleration can be expected when the angle of impact is around 35°. This helps other 266 researchers or tester to know at what range of angles should expect the highest rotational acceleration, and 267 consequently the most severe head injury due to the rotational acceleration. For example, one can test a 268 helmeted headform at 4.5 m/s and 7.4 m/s and interpolate the results to find the helmeted headform's 269 performance at the speeds in between without performing the test. Also, one can test a helmeted headform 270 at different angles, fixing the speed, and extrapolate the data to find the helmeted headform's performance 271 at different speeds without performing the test.

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#### 275 REFERENCES

- Aare, M. & Halldin, P., 2003. A new laboratory rig for evaluating helmets subject to oblique impacts.
- 277 Traffic Injury Prevention, 4(3), pp. 240-248.
- Aare, M., Kleiven, S. & Halldin, P., 2004. Injury tolerances for oblique impact helmet testing. IJCrash,
  9(0), pp. 000-000.
- Abram, D. E., Golnaraghi, F. & Wang, G. G., 2018. Suspension-based Impact System. Patent No.
- 281 62/636732.
- Abram, D. E., Wikarna, A., Golnaraghi, F. & Wang, G., 2019. A Modular Impact Diverting Mechanism
  for Football Helmets. *Journal of Biomechanics*.
- Bartsch, A. et al., 2012. Hybrid III anthropomorphic test device (ATD) response to head impacts and
- potential implications for athletic headgear testing. Accident Analysis and Prevention, Volume 48, pp.
  285 285-291.
- Bland, M. L., McNally, C. & Rowson, S., 2018. STAR Methodology for Bicycle Helmets, Blacksburg,
  VA: Virginia Tech, Virginia Tech Helmet Lab.
- Bliven, E. et al., 2019. Evaluation on a Novel Bicycle Helmet Concept in Oblique Impact Testing. *Accident Analysis and Prevention*, Volume 124, pp. 58-65.
- 291 Brolinson, P. G. et al., 2006. Analysis of Linear Head Accelerations from Collegiate Football Impacts.
- 292 Current Sports Medicine Reports, January, 5(1), pp. 23-28.
- 293 Camacho, D. L. et al., 1997. Experimental Flexibility Measurements for the Development of a
- 294 computational Head-Neck Model Validated for Near-Vertex Head Impact. SAE 973345.
- 295 Chinn, B. et al., 2001. COST 327 Motorcycle Safety Helmet, Luxembourg: Office for Official
- 296 Publications of the European Communities.
- 297 Cobb, B. R. et al., 2015. Quantitative Comparison of Hybrid III and NOCSAE Headform Shape
- 298 Characteristics and Implications on Football Helmet Fit. Proc. Inst. Mech. Eng., Part P, pp. 39-46.
- 299 Consumer Product Safety Commission, 1998. Safety Standard for Bicycle Helmets; Final Rule, 16 CFR
- 300 Part 1203, s.l.: s.n.

- 301 Cripton, P. A. et al., 2014. Bicycle helmets are highly effective at preventing head injury during head
- 302 impact: Head-form accelerations and injury criteria for helmeted and unhelmeted impacts. Accident
- 303 Analysis and Prevention, Volume 70, pp. 1-7.
- 304 Crisco, J. J. et al., 2010. Frequency and location of head impact exposures in individual collegiate football
- 305 players. Journal of Athletic Training, 45(6), pp. 549-559.
- 306 Daniel, R., Rowson, S. & Duma, S., 2012. Head impact exposure in youth football. Annals of Biomedical
- 307 Engineering, 40(4), pp. 976-981.
- 308 Deck, C. et al., 2012. Proposal of an improved bicycle helmet standards. Politecnico Milano, s.n.
- 309 Deck, C. & Willinger, R., 2008. Improved head injury criteria based on head FE model. Int J Crash,
- 310 Volume 13, pp. 667-679.
- 311 DeMarco, A. L. et al., 2010. The impact response of motorcycle helmets at different impact severities.
- 312 Accident Analysis and Prevention, Volume 42, pp. 1778-1784.
- 313 DeMarco, A. L., Chimich, D. D., Gardiner, J. C. & Siegmund, G. P., 2016. The impact response of
- traditional and BMX-style bicycle helmets at different impact severities. Accident Analysis and
- 315 Prevention, Volume 92, pp. 75-183.
- 316 Ebrahimi, I., Golnaraghi, F. & Wang, G. G., 2015. Factors Influencing the oblique impact test of
- 317 motorcycle helmets. Traffic Injury Prevention, 16(4), pp. 404-408.
- Fernandes, F. A. & Alves de Sousa, R. J., 2013. Finite element analysis of helmeted oblique impacts and
  head injury evaluation with a commercial road helmet. Structural Engineering and Mechanics, 48(5), pp.
  661-679.
- Finan, J. D., Nightingale, R. W. & Myers, B. S., 2008. The Influence of Reduced Friction on Head Injury
  Metrics in Helmeted Head Impacts. *Traffic Injury Prevention*, 9(5), pp. 483-488.
- 323 Gwin, J. T. et al., 2009. An Investigation of the NOCSAE Linear Impactor Test Method Based on In Vivo
- 324 Measures of Head Impact Acceleration in American Football. Journal of Biomechanical Engineering,
- 325 132(1).
- Halldin, P., Aare, M., Kleiven, S. & von Holst, H., 2003. Improved helmet design and test methods to
- 327 reduce rotational induced brain injuries. s.l., RTO Specialist Meeting, the NATO's Research and
- 328 Technology Organization (RTO).

- 329 Halldin, P., 2015. CEN/TC 158 Working Group 11 Rotational Test Methods-Proposal for a New Test
- 330 Method Measuring the Kinematics in Angled Helmeted Impacts, s.l.: s.n.
- Halldin, P. & Kleiven, S., 2013. The Development of Next Generation Test Standards for Helmets.
- 332 London, s.n.
- 333 Herbst, B., Forrest, S. & Chang, D., 1998. Fidelity of Anthropometric Test Dummy Necks in Rollover
- 334 Accidents. Windsor, ON, Canada, s.n.
- 335 Hodgson, V. & Thomas, L., 1971. Comparison of Head Acceleration Injury Indices in Cadaver Skull
- 336 Fracture. SAE Technical Paper 710854.
- Holburn, A. H. S., Edin, M. A. & Oxfd, D. P., 1943. Mechanics of Head Injuries. The Lancet, Volume
  242, pp. 438-441.
- 339 Hoshizaki, B., Vassilyadi, M., Post, A. & Oeur, A., 2012. Performance Analysis of Winter Activity
- Protection Headgear for Young Children: Laboratory Investigation. J. Neurosurg. Pediatr., 9(2), pp. 133138.
- 342 Ivancic, P. C., 2014. Cervical spine instability following axial compression injury: A biomechanical
- 343 study. Orthopaedics & Traumatology: Surgery & Research, Volume 100, pp. 127-133.
- 344 King, A. I., Yang, K. H., Zhang, L. & Hardy, W., 2003. Is Head Injury Caused by Linear or Angular
- 345 Acceleration?. Lisbon, Portugal, s.n.
- 346 Kleiven, S., 2013. Why Most Traumatic Brain Injuries are Not Caused by Linear Acceleration but Skull
- 347 Fractures are. Frontiers in Bioengineering and Biotechnology, Volume 1, pp. 1-5.
- 348 Kuramochi, R. et al., 2004. Anticipatory modulation of neck muscle reflex responses induced by
- 349 mechanical perturbations of the human forehead. Neuroscience letters, Volume 366, pp. 206-210.
- MacAlister, A., 2013. Surrogare Head Forms for the Evaluation of Head Injury Risk. Brain Injuries andBiomechanics.
- 352 McElhaney, J. H., Roberts, V. L., Hilyard, J. F. & Kenkyūjo, N. J., 1976. Properties of human tissues and
- components: nervous tissues. In: Handbook of human tolerance. Tokyo: Japan, p. 143.
- 354 Mills, N. J., Wilkes, S., Derler, S. & Flisch, A., 2009. FEA of Oblique Impact Test on a Motorcycle
- Helmet. International Journal of Impact Engineering, Volume 36., pp. 913-925.
- 356 Myers, B. S. et al., 1989. Response of the Human Cervical Spine to Torsion. Washington, DC, s.n.

- 357 Nightingale, R. W., McElhaney, J. H., Richardson, W. J. & Myers, B. S., 1996. Dynamic Responses of
- the Head and Cervical Spine to Axial Impact Loading. J. Biomechanics, 29(3), pp. 307-318.
- 359 Noble, J. M. & Hesdorffer, D. C., 2013. Sport-Related Concussions: A Review of Epidemiology,
- 360 Challenges in Diagnosis, and Potential Risk Factors. Neuropsychol Rev, Volume 23, pp. 273-284.
- 361 NOCSAE, DOC, 2016. Standard Performance Specification for Newly Manufactured Ice Hockey
- 362 Helmets, Overland Park: National Operating Committee on Standards For Athletic Equipment.
- 363 NOCSAE, DOC, 2017. Standard Test Method and Equipment Used in Evaluating The performance
- 364 Characteristics of Headgear/Equipment, Overland Park: National Operating Committee on Standards for
- 365 Athletic Equipment.
- 366 NOCSAE, DOC, 2019. Standard Performance Specification for Newly Manufactured Football Helmets,
- 367 Overland Park: National Operating Committee on Standards For Athletic Equipment.
- 368 Ono, K. et al., 2003. Biomechanical response of the head, neck, and torso to direct impact on the back of
- 369 male and female volunteers. Lisbon, s.n.
- 370 Otte, D., 1991. Technical demands on safety in the design of crash helmets for biomechanical analysis of
- 371 real accident situations. SAE Technical Paper 912911.
- 372 Padgaonkar, A. J., Krieger, K. W. & King, A. I., 1975. Measurement of angular acceleration of a rigid
- body using linear accelerometers. J. Appl. Mech., 42(3), pp. 552-556.
- Pellman, E. J. et al., 2003. Concussion in professional football: reconstruction of game impacts and
- 375 injuries part 1. Neurosurgery, 53(4), pp. 799-814.
- 376 Pellman, E. et al., 2003. Concussion in professional football: location and direction of helmet impacts -
- 377 Part 2. Neurosurgery, 53(6), pp. 1328-1341.
- Post, A. et al., 2017. The Effect of Acceleration Signal Processing for Head Impact Numeric Simulation.
- 379 Sports Eng, 20(2), pp. 111-119.
- 380 Rowson, B., Rowson, S. & Duma, S., 2015. Hockey STAR: A Methodology for Assessing the
- Biomechanical Performance of Hockey Helmets. Annals of Biomedical Engineering, 10(2429-2443), p.
- 382 43.
- 383 Rowson, S., Daniel, R. W. & Duma, S. M., 2013. Biomechanical performance of leather and modern
- football helmets. J Neurosurg, Volume 119, pp. 805-809.

- Rowson, S. & Duma, S., 2011. Development of the STAR Evaluation System for Football Helmets:
- 386 Integrating Player Head Impact Exposure and Risk of Concussion. Annals of Biomedical Engineering,
- 387 39(8), pp. 2130-2140.
- 388 Sone, J. Y., Kondziolka, D., Huang, J. H. & Uzma, S., 2016. Helmet efficacy against concussion and
- traumatic brain injury: a review. Journal of Neurosurgery, 126(3), pp. 1-14.
- 390 Svensson, M. Y. & Lovsund, P., 1992. A Dummy for Rear-End Collisions Development and Validation
- 391 of a New Dummy-Neck. Verona, Italy, s.n.
- Trotta, A. et al., 2018. Evaluation of The Head-Helmet Sliding Properties in an Impact Test. Journal of
  Biomechanics, Volume 75, pp. 28-34.
- 394 UN ECE Regulation 22/05, 2002. Uniform Provisions Concerning The Approval of Protective Helmets
- and Their Visors for Drivers and Passengers of Motor Cycles and Mopeds, Geneva: s.n.
- Vastag, B., 2002. Foorball brain injuries draw increased scrutiny. JAMA Jan. 23-30, 287(4), pp. 437-439.
- 397 Whyte, T. et al., 2019. A Review of Impact Testing Methods for Headgear in Sports: Considerations for
- 398 Improved Prevention of Head Injury Through Research and Standards. Journal of Biomechanical
- 399 Engineering, 141(7).
- Willinger, R. & Baumgartner, D., 2003. Human head tolerance limits to specific injury mechanism.
  IJCrash, 8(6), pp. 605-617.
- Willinger, R. et al., 2015. Final Report of Working Group 3: Impact Engineering, Brussels, Belgium:
  OCST Action TU1101/HOPE.
- 404 Zhang, L., Yang, K. H. & King, A. I., 2004. A proposed injury threshold for mild traumatic brain injury.
- 405 Journal of Biomedical Engineering, Volume 126, pp. 226-236.
- 406